

DNA Detection by Solid-State UV Sensors

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State-of-the-art DNA sensors Labelleld techniques

labelling imposes extratime and cost demands; **can interfere** with the molecular interaction (false negative); **background** binding(positive negative)

Fluorescence Microarrays

high-density (390000sites/cm² for in-situ synthesis of short oligonucleotides)
very high-sensitivity (1 pM single-molecule-fluorescence)

Electrochemical Biosensors

- Iow-density
- very-high sensitivity (10 pM)
- some drift issues

degree of development: Research and laboratory applications

Label-free techniques

Surface Plasmon Resonance

Mass sensors (QCM, SAW and cantilevers)

- very limited number of sites: problems of addressability and implementation
- good sensitivity (1 nM SPR), (QCM 50 nM)
- no background signal, no sample pollution...

degree of development: Research and laboratory equipment (QCM and SPR)

Role of Technology and Electronics

- Microfabrication and Photolithography
 - High-density patterns for molecular sites
 - Integration of microfluidic, thermal and mechanical functions on chip
- Semiconductor sensors (solid-state devices) for electronic transduction of molecular interactions
- Realization of measurements systems (embedded, SoB, SoC...) for signal detection, conditioning, processing

Can lead to

High-parallel, High-perfomance, Mass-Produced DNA sensors

Our Approach. Label-free Techniques

Labeled (Indirect)



Label-free (Direct) Techniques

1- Electrical technique

Changes in the capacitive behavior of an electrode/solution bio-sensing interface **Electronics**: development of a measurement system based on integrable capacitive measurement circuit **Microfabrication**: test of the technique on microfabricated electrodes

2 – Optical Technique molecular UV-absorbance Semiconductor sensors:

- 'ad hoc' high-sensitive amorphous silicon photodiodes
- Non-volatile memory cells

Charge-Based Capacitance Measurement Circuit

Advantages vs. standard complex impedance meters

very simple, easily integrable

 the analog part can be reduced to an I/V and an A/D converter

Non Complementary





Microfabricated electrodes

Challenges: 1- Stability of electrode capacitance in solution 2- Adapted passivation **3- Integration with** microfuidics

Total measured capacitance ($2 \times 10^{-3} \mu m^2$): between 100 pF and 1 nF sample deposition and

Percentage decrease of Capacitance after rinsing



Sample		
Complementary sequence	37.7	
Complementary		
sequence	18.3	
Complementary		
sequence	29.5	
Non		
Complementary		
Sequence	-5.2	
DNA-free sample	-6.2	
DNA-free sample	-3.7	
DNA-sample on		
bare electrode	1.8 6	

UV molecular absorbance

 UV spectroscopy for molecular quantification and detection of molecular interactions

Amorphous Silicon UV sensor

In collaboration with Università La Sapienza di Roma G. De Cesare, D. Caputo, A. Nascetti

Non-volatile single-poly memory cell



Absorbance

The measurement of absorption of ultraviolet by species in solution provides one of the most widely used methods of quantitative analysis available in analytical laboratory

Lamber-Beer law: $A = \varepsilon C$

Fabrication of Amorphous Silicon devices for UV sensing

- Amorphous silicon is a low-cost material, lowtemperature deposition process (PECVD (Plasma Enhanced Chemical Vapour Deposition)
- Deposition process is compatible with several low-cost substrates on which a conductor film can be pre-deposited
- Can be fabricated on substrates of any size
- The device implementation can be tuned to improve resolution or selectivity or in the UV range.

System implementations



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I-V Characteristics

I-V light @253.4 nm and 0.5µW incident radiation



Responsivity @253.4 nm: 45mA/W

Experimental Setup



Relative current signal corresponding to DNA samples with different absorbances

30-mer; ε = 280700(L/mole*cm); MW 9208 (g/mole) Buffer TAE Mg2+



The relative current signal is derived from the measured current of the UV sensor as follows: (I_{BUFFER} - I_{DNA}) / I_{BUFFER}

I_{DNA} with oligonucleotides I_{BUFFER} buffer solutions without oligonucleotides

Minimum Absorbance for Hybridization detection



Amorphous Silicon Devices

- Minimum absorbance to resolve hypochromic effect (detect DNA hybridization)
 - theoretical: Amin = 4.6×10^{-6}
 - experimental setup : Amin = 6.8 × 10⁻⁴, which corresponds to 2.43 nM concentration for 1 cm pathlength and a 30-mer oligonucleotide (suitable for PCR-amplified strands)
- Eximated Absorbance of immobilized DNA layers: A ≈ 10⁻³ ⇒ DNA detection can be achieved with the present set-up

Non-volatile memory Cell

Standard EPROM cell

UV are used to lower the threshold voltage V_{TH} by extracting electrons previously injected into the Floating Gate



EPROM cell single-poly better exposition to UV ligth

extended floating gate surfaceexposed floating gate



Memory Cell Characterization



Experimental Results

Expected concentration for a DNA layer 10 nM



DNA in buffer solution (bulk) 30-mer; ε = 280700(L/mole*cm); MW 9208 (g/mole) Buffer TAE Mg2+

Comparison between Amorphous Silicon Detectors and EPROM memory cell

EPROM memory cell

Amorphous Silicon Detectors

easy implementation of high-density chips

high-cost implementation/materials

good sensitivity in the nanomolar range

 high-density and large surface

 low-cost implementation materials

 high resolution on the sub-nanomolar range with enhanced stability in integrated set-up

